



Introduction to Inverse Problems

Bastian von Harrach

`harrach@math.uni-stuttgart.de`

Chair of Optimization and Inverse Problems, University of Stuttgart, Germany

Department of Computational Science & Engineering
Yonsei University

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Motivation and examples

Laplace's demon

Laplace's demon: *(Pierre Simon Laplace 1814)*

"An intellect which (...) would know all forces (...) and all positions of all items (...), if this intellect were also vast enough to submit these data to analysis, (...); for such an intellect nothing would be uncertain and the future just like the past would be present before its eyes."





Computational Science

Computational Science / Simulation Technology:

If we know all necessary parameters, then we can numerically predict the outcome of an experiment (by solving mathematical formulas).

Goals:

- ▶ Prediction
- ▶ Optimization
- ▶ Inversion/Identification

Computational Science

Generic simulation problem:

Given input x calculate outcome $y = F(x)$.

$x \in X$: parameters / input

$y \in Y$: outcome / measurements

$F: X \rightarrow Y$: functional relation / model

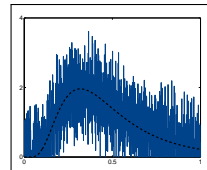
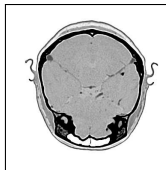
Goals:

- **Prediction:** Given x , calculate $y = F(x)$.
- **Optimization:** Find x , such that $F(x)$ is optimal.
- **Inversion/Identification:** Given $F(x)$, calculate x .

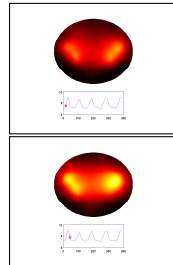
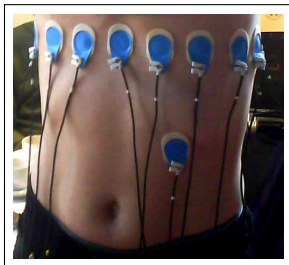
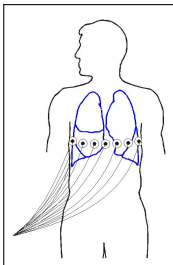
Examples

Examples of inverse problems:

- ▶ Electrical impedance tomography
- ▶ Computerized tomography
- ▶ Image Deblurring
- ▶ Numerical Differentiation

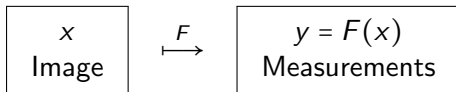


Electrical impedance tomography (EIT)



- ▶ Apply electric currents on subject's boundary
- ▶ Measure necessary voltages
- Reconstruct conductivity inside subject.

Electrical impedance tomography (EIT)



x : Interior conductivity distribution (image)

y : Voltage and current measurements

Direct problem: Simulate/predict the measurements
(from knowledge of the interior conductivity distribution)
Given x calculate $F(x) = y!$

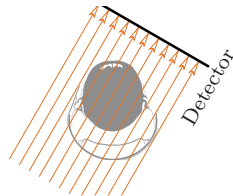
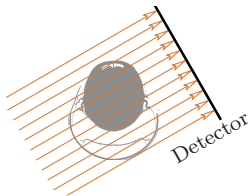
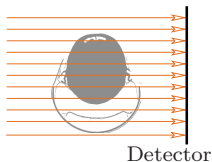
Inverse problem: Reconstruct/image the interior distribution
(from taking voltage/current measurements)
Given y solve $F(x) = y!$

X-ray computerized tomography

Nobel Prize in Physiology or Medicine 1979:
Allan M. Cormack and Godfrey N. Hounsfield
(Photos: Copyright ©The Nobel Foundation)



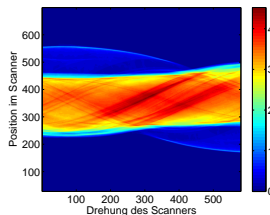
Idea: Take x-ray images from several directions



Computerized tomography (CT)



Image



Measurements

Direct problem:

Simulate/predict the measurements

(from knowledge of the interior density distribution)

Given x calculate $F(x) = y!$

Inverse problem:

Reconstruct/image the interior distribution

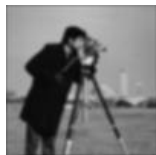
(from taking x-ray measurements)

Given y solve $F(x) = y!$

Image deblurring


 x

True image


 $y = F(x)$

Blurred image

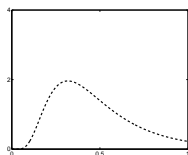
Direct problem: Simulate/predict the blurred image
(from knowledge of the true image)

Given x calculate $F(x) = y!$

Inverse problem: Reconstruct/image the true image
(from the blurred image)

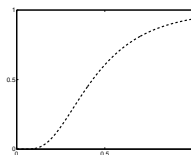
Given y solve $F(x) = y!$

Numerical differentiation


 x

Function

 F


 $y = F(x)$

Primitive Function

Direct problem:

Calculate the primitive

Given x calculate $F(x) = y$!

Inverse problem:

Calculate the derivative

Given y solve $F(x) = y$!



Ill-posedness



Well-posedness

Hadamard (1865–1963): A problem is called **well-posed**, if

- ▶ a solution exists,
- ▶ the solution is unique,
- ▶ the solution depends continuously on the given data.

Inverse Problem: *Given y solve $F(x) = y$!*

- ▶ F surjective?
- ▶ F injective?
- ▶ F^{-1} continuous?

Ill-posed problems

Ill-posedness: $F^{-1} : Y \rightarrow X$ not continuous.

$\hat{x} \in X$: true solution

$\hat{y} = F(\hat{x}) \in Y$: exact measurement

$y^\delta \in Y$: real measurement containing noise $\delta > 0$,

e.g. $\|y^\delta - \hat{y}\|_Y \leq \delta$

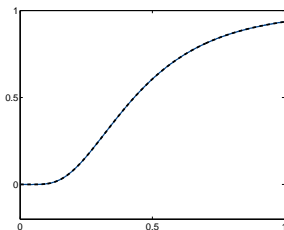
For $\delta \rightarrow 0$

$$y^\delta \rightarrow \hat{y}, \quad \text{but (generally)} \quad F^{-1}(y^\delta) \not\rightarrow F^{-1}(\hat{y}) = \hat{x}$$

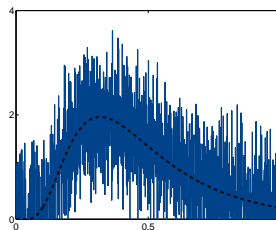
Even the smallest amount of noise will corrupt the reconstructions.

Numerical differentiation

Numerical differentiation example ($h = 10^{-3}$)



$y(t)$ and $y^\delta(t)$



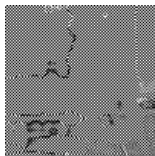
$\frac{y(t+h)-y(t)}{h}$ and $\frac{y^\delta(t+h)-y^\delta(t)}{h}$

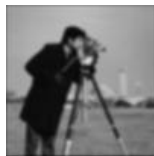
Differentiation seems to be an ill-posed (inverse) problem.

Image deblurring



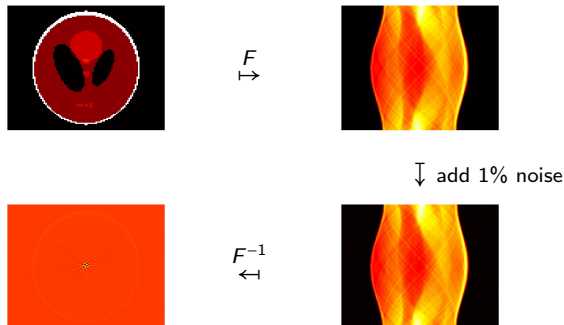
$$F \mapsto$$


$$\downarrow \text{ add 0.1\% noise}$$


$$F^{-1} \leftarrow$$


Deblurring seems to be an ill-posed (inverse) problem.

Image deblurring



CT seems to be an ill-posed (inverse) problem.



Compactness and ill-posedness

Compactness

Consider the general problem

$$F : X \rightarrow Y, \quad F(x) = y$$

with X, Y real Hilbert spaces.

Assume that F is linear, bounded and injective with left inverse

$$F^{-1} : F(X) \subseteq Y \rightarrow X.$$

Definition 1.1. $F \in \mathcal{L}(X, Y)$ is called **compact**, if

$\overline{F(U)}$ is compact for alle bounded $U \subseteq X$,

i.e. if $(x_n)_{n \in \mathbb{N}} \subset X$ is a bounded sequence then $(F(x_n))_{n \in \mathbb{N}} \subset Y$ contains a bounded subsequence.



Compactness

Theorem 1.2. Let

- ▶ $F \in \mathcal{L}(X, Y)$ be compact and injective, and
- ▶ $\dim X = \infty$,

then the left inverse F^{-1} is not continuous, i.e. the inverse problem

$$Fx = y$$

is ill-posed.



Compactness

Theorem 1.3. Every limit¹ of compact operators is compact.

Theorem 1.4. If $\dim \mathcal{R}(F) < \infty$ then F is compact.

Corollary. Every operator that can be approximated¹ by finite dimensional operators is compact.

¹in the uniform operator topology



Compactness

Theorem 1.5. Let $F \in \mathcal{L}(X, Y)$ possess an unbounded left inverse F^{-1} , and let $R_n \in \mathcal{L}(Y, X)$ be a sequence with

$$R_n y \rightarrow F^{-1} y \quad \text{for all } y \in \mathcal{R}(F).$$

Then $\|R_n\| \rightarrow \infty$.

Corollary. If we discretize an ill-posed problem, the better we discretize, the more unbounded our discretizations become.



Compactness and ill-posedness

Discretization: Approximation by finite-dimensional operators.

Consequences for discretizing infinite-dimensional problems:

If an infinite-dimensional direct problem can be discretized¹, then

- ▶ the direct operator is compact.
- ▶ the inverse problem is ill-posed, i.e. the smallest amount of measurement noise may completely corrupt the outcome of the (exact, infinite-dimensional) inversion.

If we discretize the inverse problem, then

- ▶ the better we discretize, the larger the noise amplification is.

¹in the uniform operator topology



Examples

- ▶ The operator

$$F: \text{function} \mapsto \text{primitive function}$$

is a linear, compact operator.

↷ The inverse problem of differentiation is ill-posed.

- ▶ The operator

$$F: \text{exact image} \mapsto \text{blurred image}$$

is a linear, compact operator.

↷ The inverse problem of image deblurring is ill-posed.



Examples

- ▶ In computerized tomography, the operator

$$F : \text{image} \mapsto \text{measurements}$$

is a linear, compact operator.

↷ The inverse problem of CT is ill-posed.

- ▶ In EIT, the operator

$$F : \text{image} \mapsto \text{measurements}$$

is a non-linear operator. Its Fréchet derivative is a compact linear operator.

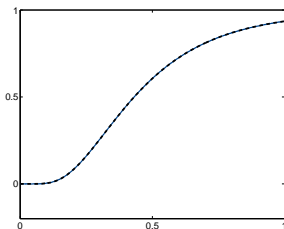
↷ The (linearized) inverse problem of EIT is ill-posed.



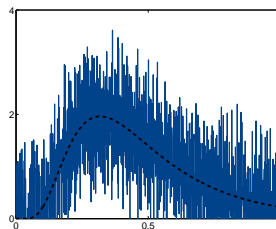
Regularization

Numerical differentiation

Numerical differentiation example



$y(t)$ and $y^\delta(t)$



$\frac{y(t+h)-y(t)}{h}$ and $\frac{y^\delta(t+h)-y^\delta(t)}{h}$

Differentiation is an ill-posed (inverse) problem

Regularization

Numerical differentiation:

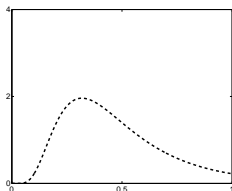
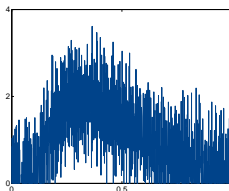
- $y \in C^2$, $C := 2 \sup_{\tau} |g''(\tau)| < \infty$, $|y^\delta(t) - y(t)| \leq \delta \quad \forall t$

$$\begin{aligned} & \left| y'(t) - \frac{y^\delta(t+h) - y^\delta(t)}{h} \right| \\ & \leq \left| y'(t) - \frac{y(t+h) - y(t)}{h} \right| \\ & \quad + \left| \frac{y(t+h) - y(t)}{h} - \frac{y^\delta(t+h) - y^\delta(t)}{h} \right| \\ & \leq Ch + \frac{2\delta}{h} \rightarrow 0. \end{aligned}$$

for $\delta \rightarrow 0$ and adequately chosen $h = h(\delta)$, e.g., $h := \sqrt{\delta}$.

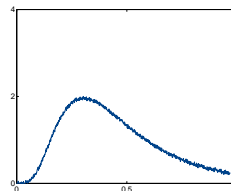
Numerical differentiation

Numerical differentiation example


 $y'(t)$


$$\frac{y^\delta(t+h) - y^\delta(t)}{h}$$

with h very small



$$\frac{y^\delta(t+h) - y^\delta(t)}{h}$$

with $h \approx \sqrt{\delta}$

Idea of regularization: Balance noise amplification and approximation

Regularization

Regularization of inverse problems:

- ▶ F^{-1} not continuous, so that generally $F^{-1}(y^\delta) \not\rightarrow F^{-1}(y) = x$ for $\delta \rightarrow 0$
- ▶ R_α continuous approximations of F^{-1}
 $R_\alpha \rightarrow F^{-1}$ (pointwise) for $\alpha \rightarrow 0$

$$R_{\alpha(\delta)} y^\delta \rightarrow F^{-1} y = x \quad \text{for } \delta \rightarrow 0$$

if the parameter $\alpha = \alpha(\delta)$ is correctly chosen.

Inexact but continuous reconstruction (regularization)
+ Information on measurement noise (parameter choice rule)
= Convergence

Prominent regularization methods

- ▶ Tikhonov regularization

$$R_\alpha = (F^*F + \alpha I)^{-1}F^*$$

- ▶ R_α continuous, $\|R_\alpha\| \leq \frac{1}{\sqrt{\alpha}}$
- ▶ $R_\alpha y \rightarrow F^{-1}y$ for $\alpha \rightarrow 0$, $y \in \mathcal{R}(F)$
- ▶ $R_\alpha y^\delta$ minimizes

$$\|F x - y^\delta\|^2 + \alpha \|x\|^2 \rightarrow \min!$$

- ▶ Truncated singular value decomposition (TSVD)
- ▶ Landweber method
- ▶ ...

Parameter choice rule

Convergence of Tikhonov-regularization

$$\|R_{\alpha}y^{\delta} - F^{-1}y\| \leq \underbrace{\|R_{\alpha}(y^{\delta} - y)\|}_{\leq \|R_{\alpha}\|\delta} + \underbrace{\|R_{\alpha}y - F^{-1}y\|}_{\rightarrow 0 \text{ for } \alpha \rightarrow 0}$$

Choose $\alpha(\delta)$ such that (for $\delta \rightarrow 0$)

- $\alpha(\delta) \rightarrow 0$
- $\|R_{\alpha(\delta)}\| \delta = \frac{\delta}{\sqrt{\alpha(\delta)}} \rightarrow 0$

then $R_{\alpha(\delta)}y^{\delta} \rightarrow F^{-1}y$. E.g., set $\alpha(\delta) := \delta$.

Exakt inversion does not converge, $F^{-1}y^{\delta} \not\rightarrow F^{-1}y$.

Tikhonov-regularization converges, $R_{\delta}y^{\delta} \rightarrow F^{-1}y$.

Better parameter choice rule:

Choose α such that $\|FR_{\alpha}y^{\delta} - y^{\delta}\| \approx \delta$ (discrepancy principle)

Image deblurring



$$\hat{x}$$



$$\hat{y} = F\hat{x}$$



$$y^\delta$$



$$F^{-1}y^\delta$$

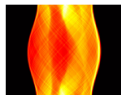


$$(F^*F + \delta I)^{-1}F^*y^\delta$$

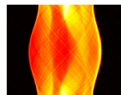
Computerized tomography



$$\hat{x}$$



$$\hat{y} = F \hat{x}$$



$$y^\delta$$



$$F^{-1} y^\delta$$



$$(F^* F + \delta I)^{-1} F^* y^\delta$$

Conclusions and remarks

Conclusions

- ▶ Inverse problems are of great importance in comput. science.
(*parameter identification, medical tomography, etc.*)
- ▶ For ill-posed inverse problems, the best data-fit solutions generally **do not converge** against the true solution.
- ▶ The regularized solutions **do converge** against the true solution.

Strategies for non-linear inverse problems $F(x) = y$:

- ▶ First linearize, then regularize.
- ▶ First regularize, then linearize.

A-priori information

- ▶ Regularization can be used to incorporate a-priori knowledge (promote sparsity or sharp edges, include stochastic priors, etc.)